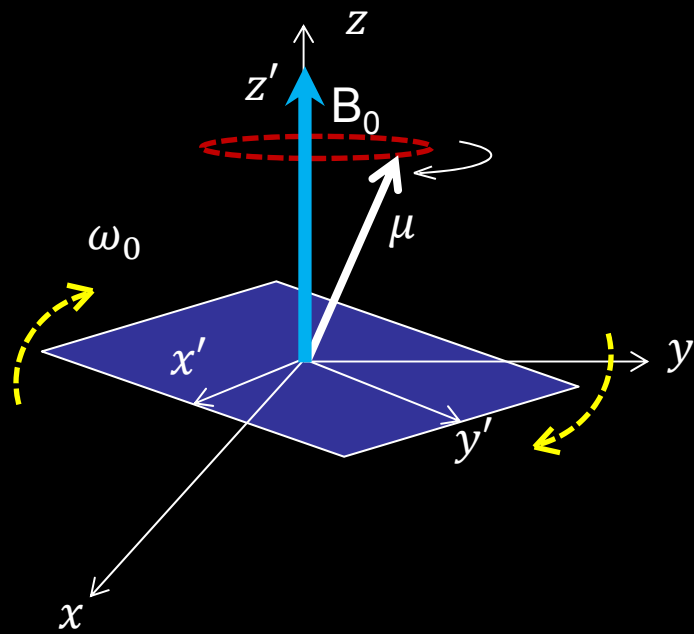


Chapter 8 – Signal acquisition Methods

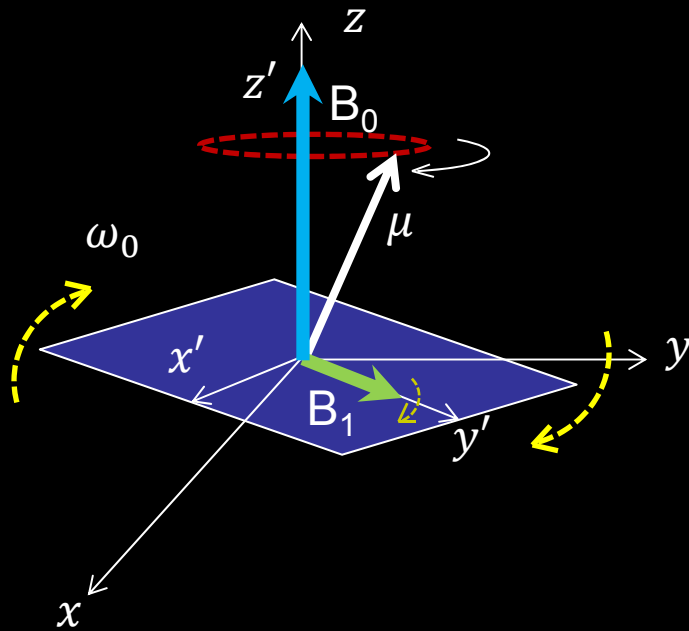
Quick Recap:



Quick Recap:

A rotating B_1 field - ON

... circularly polarized



Resonance Condition

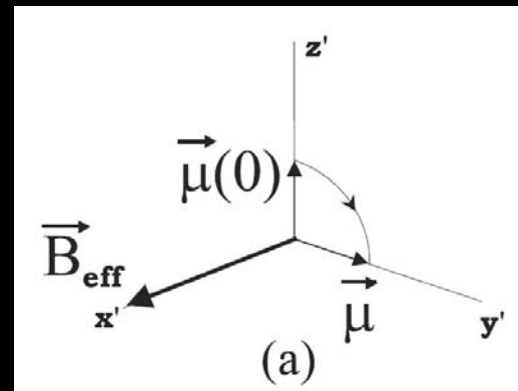
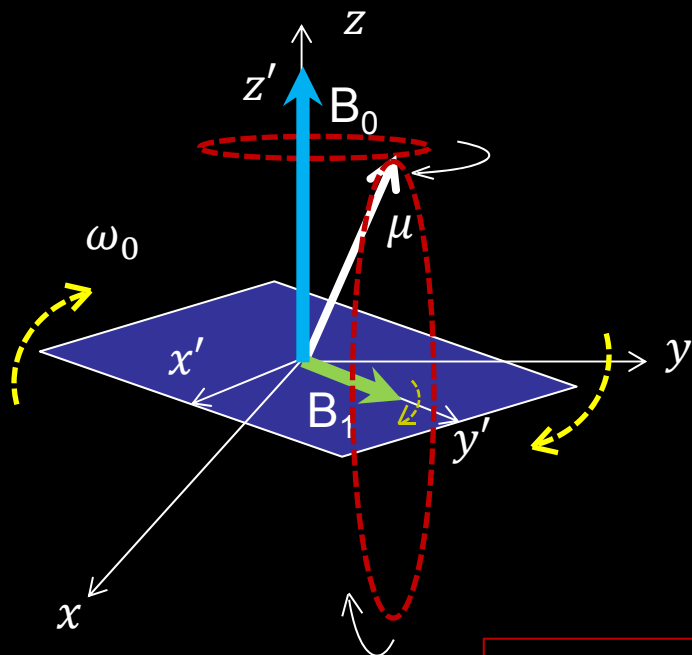
$$\omega' = \omega_0 = -\gamma \cdot B$$

$$\omega_0 = -\gamma \cdot B_0$$

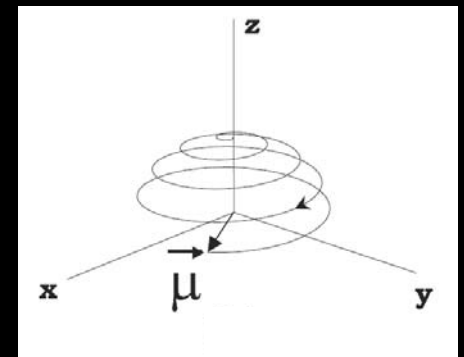
Larmor Frequency

Quick Recap:

A rotating B_1 field - ON



$$\omega_1 = -\gamma \cdot B_1$$



$$\theta = \omega_1 \cdot \tau = -\gamma \cdot B_1 \cdot \tau$$

θ – Flip angle / tipping angle

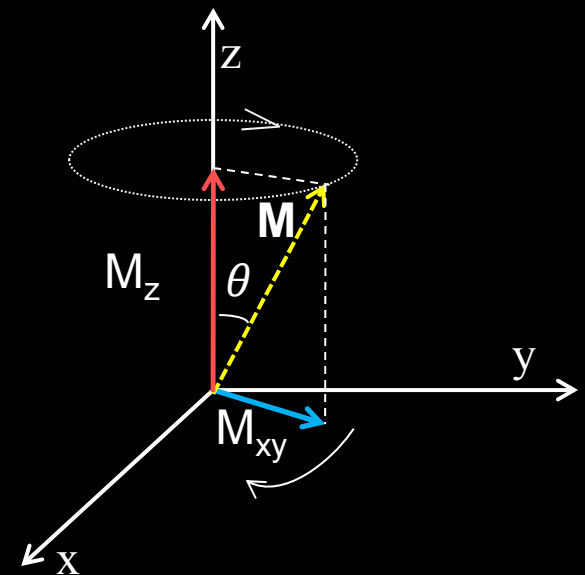
Quick Recap:

Relaxation effects

$$\frac{d\vec{M}}{dt} = \gamma \cdot \vec{M} \times B + \frac{M_0 - M_z}{T_1} - \frac{M_{xy}}{T_2}$$

M_0 is the equilibrium magnetization

M_{xy} is the transverse magnetization



Quick Recap:

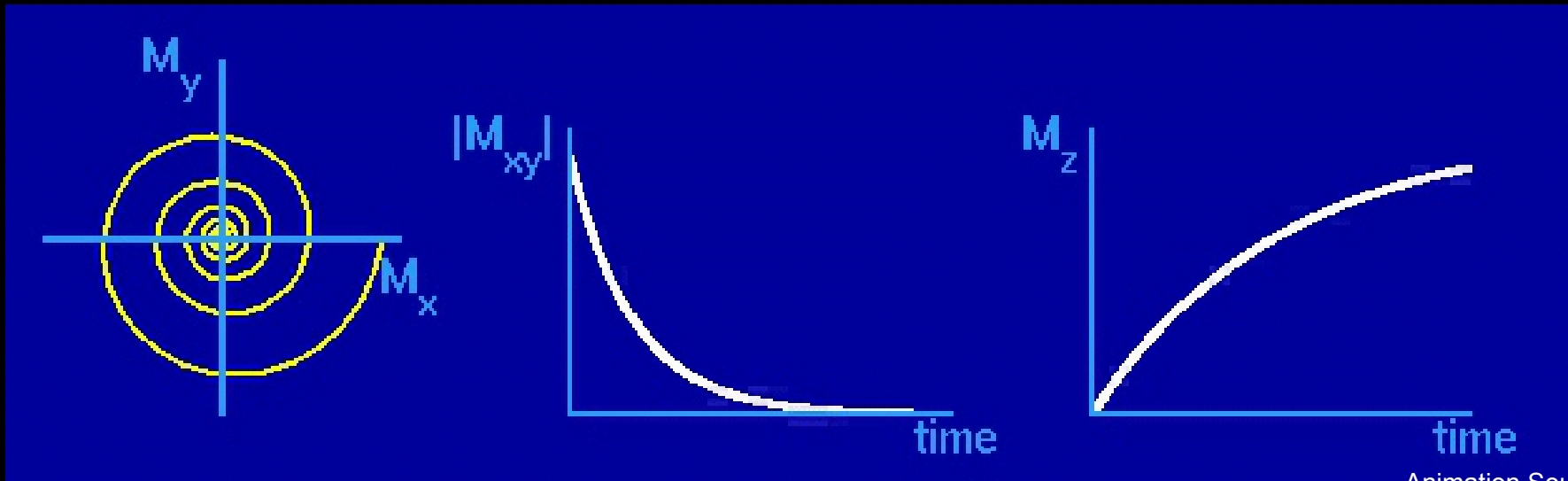
Relaxation effects

Transverse
Magnetization
Decay

$$M_{xy}(t) = M_{xy}(0) \cdot e^{-\frac{t}{T_2}}$$

Longitudinal
Magnetization
Recovery

$$M_z(t) = M_z(t=0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot \left(1 - e^{-\frac{t}{T_1}}\right)$$



Animation Source:

<http://www-mrsl.stanford.edu/~brian/intromr>

Basic Contrast Mechanisms: Relaxation effects

Longitudinal Magnetization - Recovery

$$M_z(t) = M_z(t = 0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot \left(1 - e^{-\frac{t}{T_1}}\right)$$

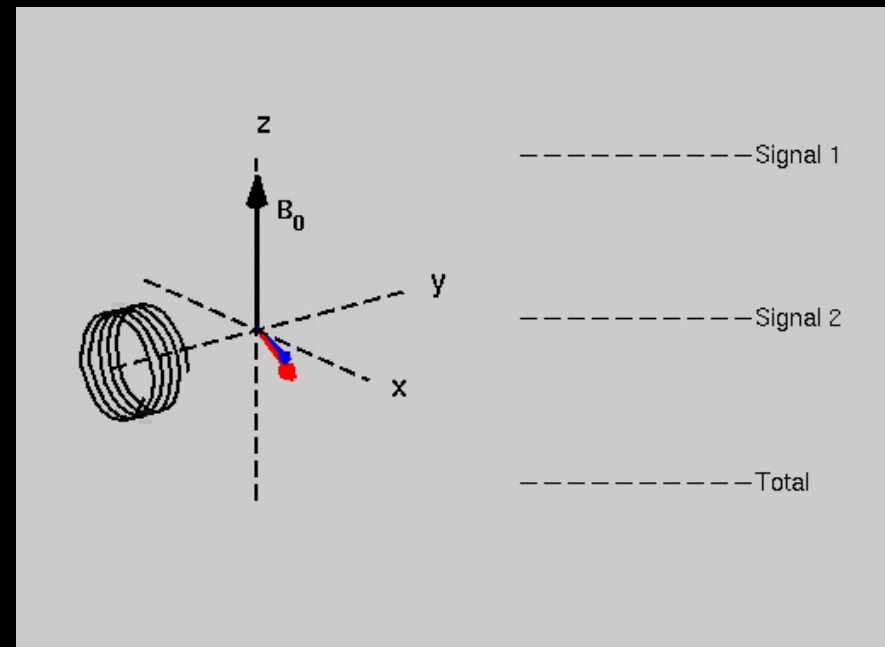
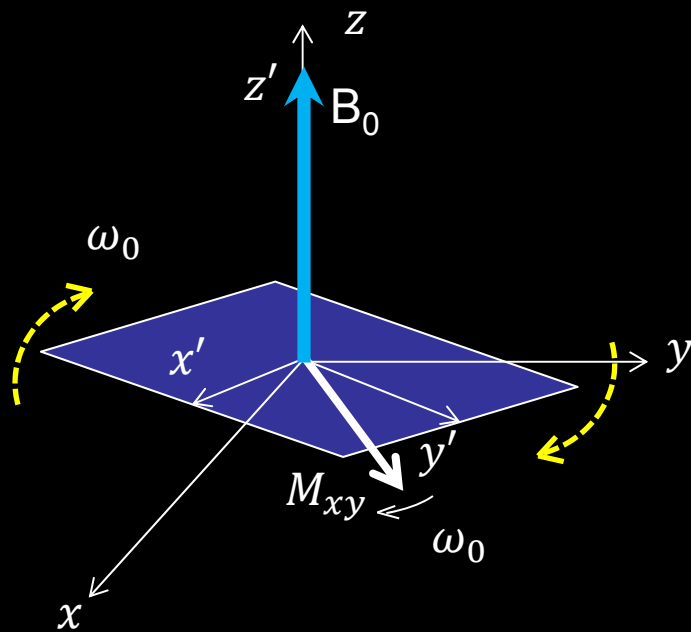
T_1 is the time it takes the magnetization to recover to 63.2% of its equilibrium value M_0 .

$$M_{xy}(t) = M_{xy}(0) \cdot e^{-\frac{t}{T_2}}$$

T_2 is the time it takes the transverse magnetization to decay to 36.7% of its initial value M_{xy} .

Quick Recap:

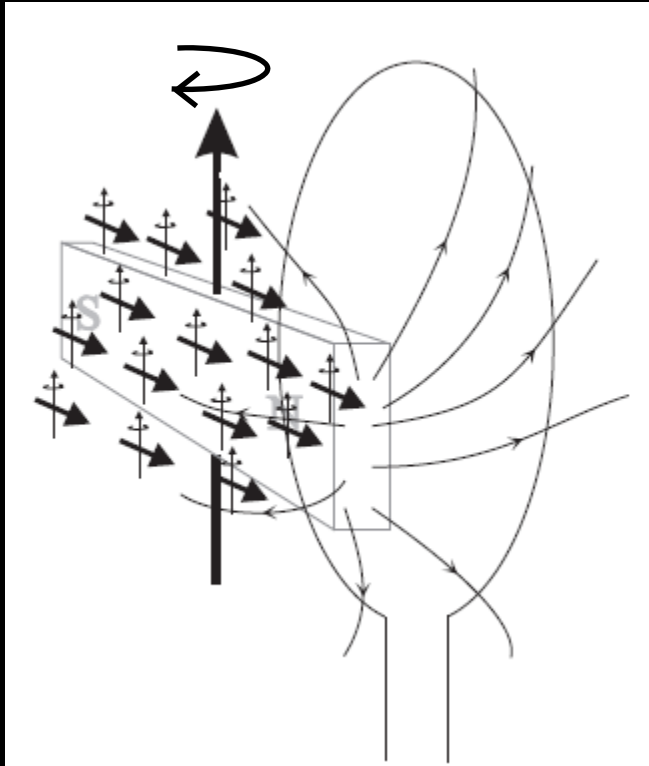
A rotating B_1 field - OFF



Quick Recap:

Signal Detection

Faraday's Law of Electromagnetic induction



$$emf = - \frac{d\Phi}{dt}$$

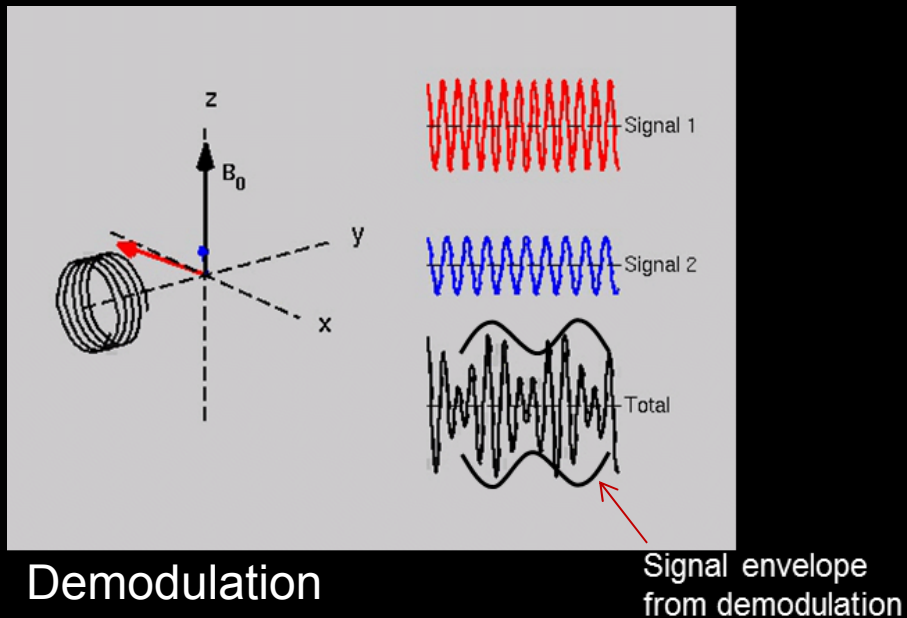
Induced signal is proportional to rate of change of flux

$$\omega_0 = -\gamma \cdot B_0$$

$$\Rightarrow emf \propto \omega_0$$

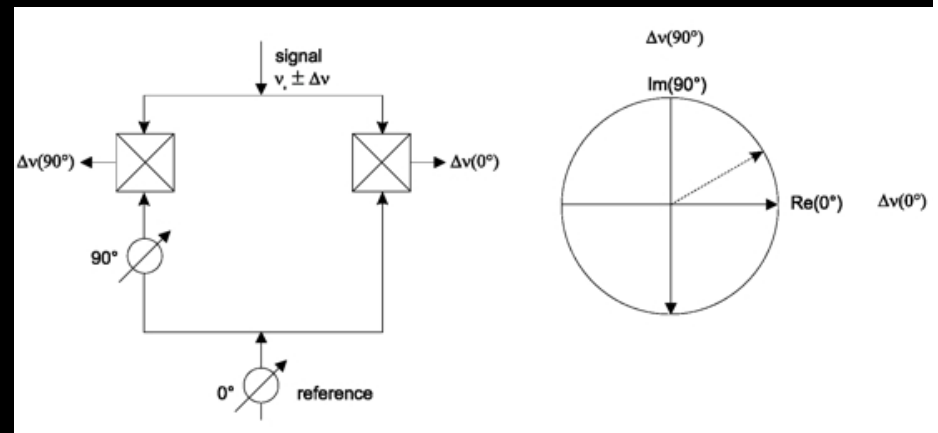
$$s(t) \propto \omega_0 \int d^3r e^{-t/T_2(\vec{r})} \mathcal{B}_\perp(\vec{r}) \underline{M_\perp(\vec{r}, 0)} e^{i(\underline{(\Omega - \omega(\vec{r}))t + \phi_0(\vec{r}) - \theta_{\mathcal{B}}(\vec{r})})}$$

Signal Demodulation and quadrature detection



Quadrature detection allows us to record both x and y components of the transverse magnetization

Quadrature detection or phase sensitive detection:



Key Points in Chapter 8

- Free Induction Decay
- Spin Echo
- Repeated rf pulse structures –
Magnetization and signal equations for different rf pulse structures

Introducing sequence timing diagram

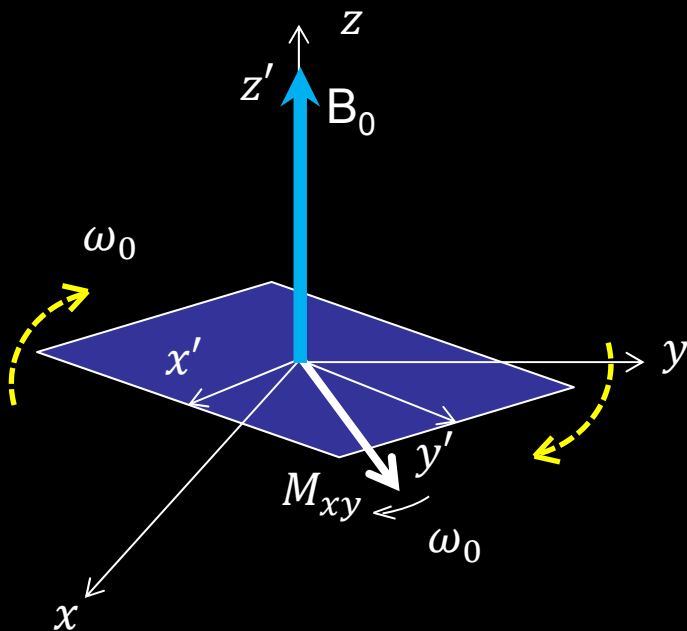
- Inversion Recovery

Demodulated Signal

$$s(t) \propto \omega_0 \int d^3r e^{-t/T_2(\vec{r})} \mathcal{B}_\perp(\vec{r}) M_\perp(\vec{r}, 0) e^{i((\Omega - \omega(\vec{r}))t + \phi_0(\vec{r}) - \theta_{\mathcal{B}}(\vec{r}))}$$

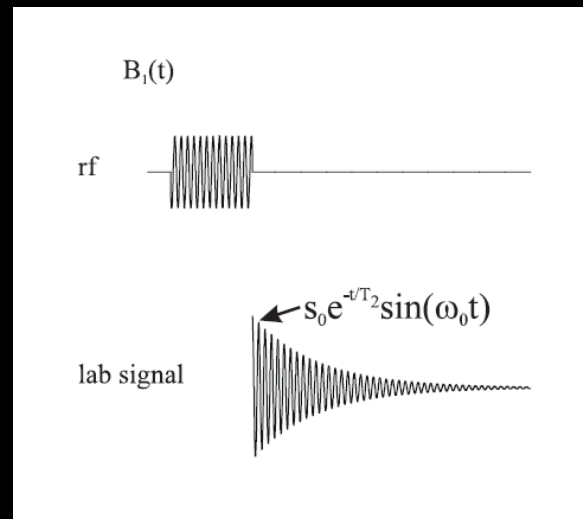
Dropping spatial dependence of T2...

$$s(t) \propto \omega_0 e^{-t/T_2} e^{i((\Omega - \omega_0)t + \phi_0 - \theta_{\mathcal{B}})} \int d^3r \mathcal{B}_\perp(\vec{r}) M_\perp(\vec{r}, 0)$$

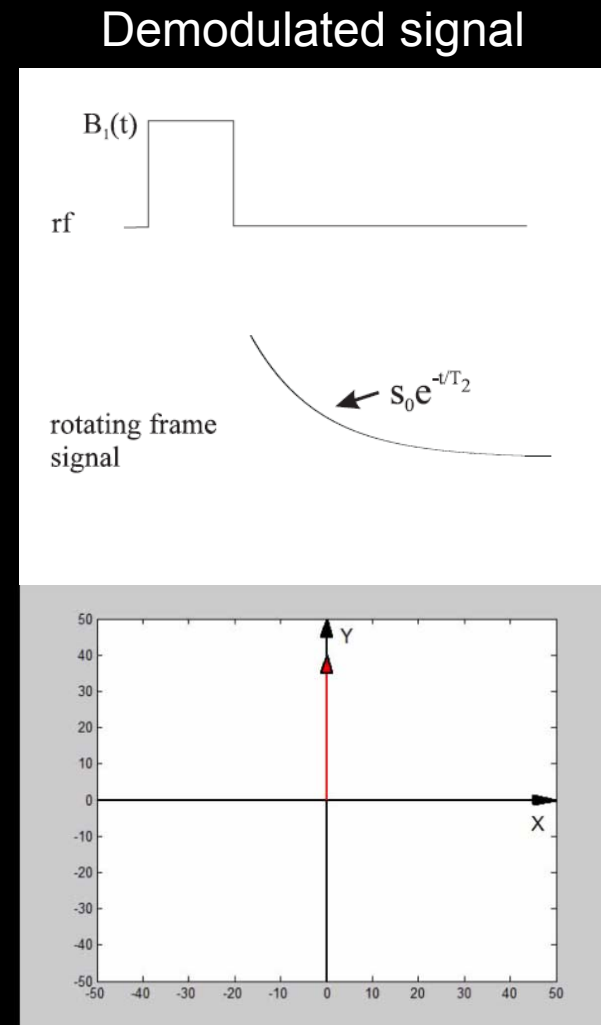


Let's assume uniform coil reception field and magnetization in the sample...

Demodulation



Laboratory reference frame



Rotating reference frame

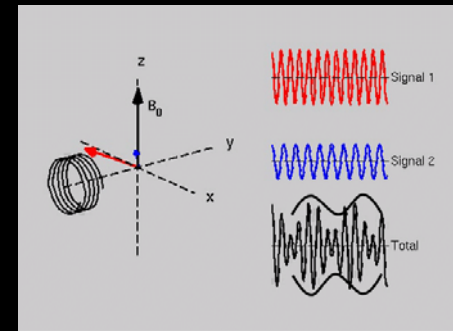
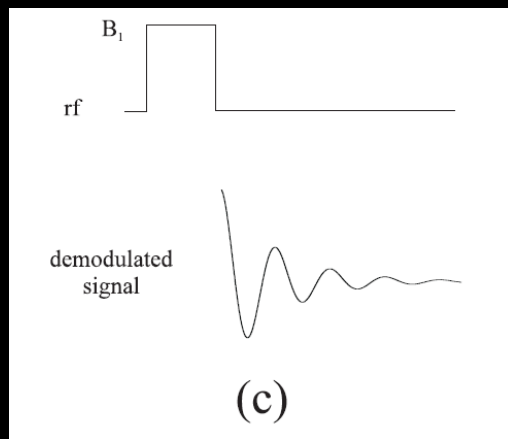
$$M_{xy} = M_0 \cdot e^{-\frac{t}{T_2}}$$

Animation Source:
Dr. Yongquan Ye, WSU

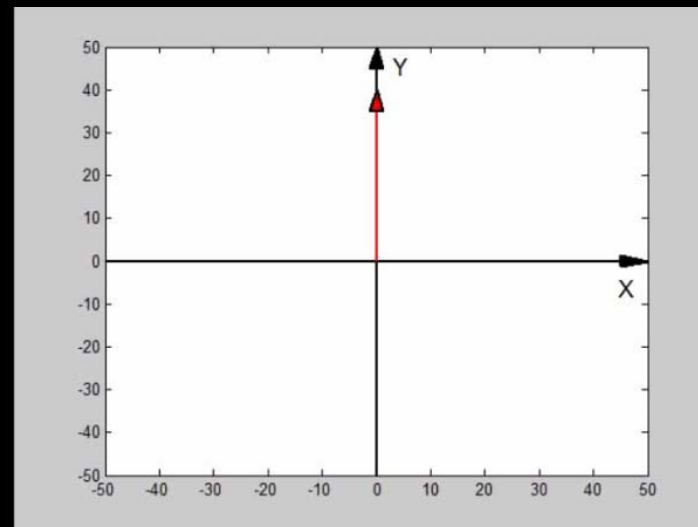
Free induction decay

$$s(t) \propto \omega_0 e^{-t/T_2} e^{i((\Omega - \omega_0)t + \phi_0 - \theta_B)} \int d^3r \mathcal{B}_\perp(\vec{r}) M_\perp(\vec{r}, 0)$$

$$\Omega \neq \omega_0 \text{ Or } \omega \neq \omega_0$$



Signal envelope from demodulation

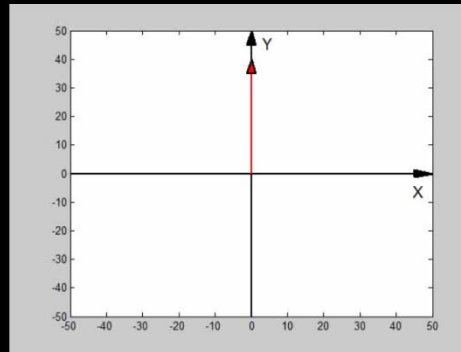
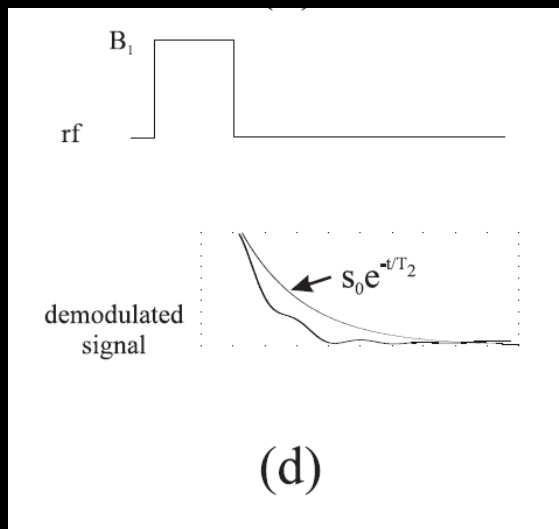


Animation Source:
Dr. Yongquan Ye, WSU

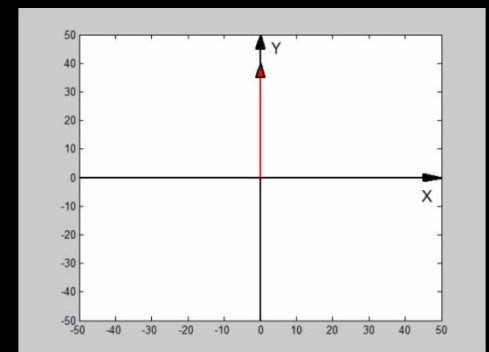
Free induction decay

Practical issue: local & global field inhomogeneity exist

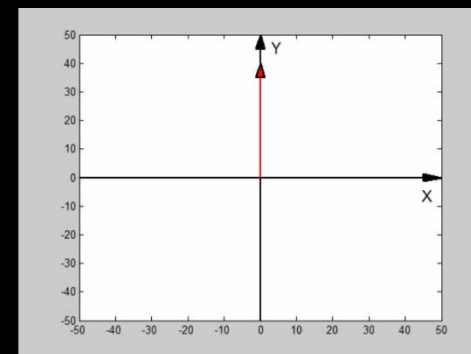
$$S(t) = S_0 \int e^{-t/T_2} e^{i(\Omega - \omega(\vec{r}))t + \phi_0}$$



90% $\Omega - \omega(\vec{r}) = 0\text{Hz}$
10% $\Omega - \omega(\vec{r}) = 50\text{Hz}$



75% $\Omega - \omega(\vec{r}) = 0\text{Hz}$
25% $\Omega - \omega(\vec{r}) = \pm 50\text{Hz}$
40 spins



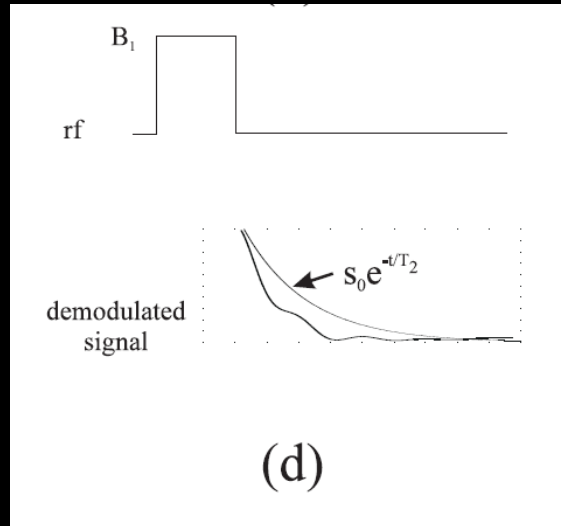
75% $\Omega - \omega(\vec{r}) = 0\text{Hz}$
25% $\Omega - \omega(\vec{r}) = \pm 50\text{Hz}$
40,000 spins

Animation Source:
Dr. Yongquan Ye, WSU

T_2^* and T_2'

Practical issue: local & global field inhomogeneity exist

$$S(t) = S_0 \int e^{-t/T_2} e^{i(\Omega - \omega(\vec{r}))t} + \phi_0$$



$$\frac{1}{T_2^*} = \frac{1}{T_2} + \frac{1}{T_2'}$$

Faster decay of signal from transverse magnetization occurs due the presence of local field inhomogeneities

*The additional decay time constant is empirically given by T_2'
($1/T_2' = R_2'$ is the additional relaxation rate)*

$$M_{xy} = M_0 \cdot e^{-\frac{t}{T_2^*}}$$

$$\begin{aligned} 1/T_2^* &= R_2^* \\ 1/T_2 &= R_2 \end{aligned}$$

$$T_2'$$

Practical issue: local & global field inhomogeneity exist

$$S(t) = S_0 \int e^{-t/T_2} e^{i(\Omega - \omega(\vec{r}))t} + \phi_0$$

The additional decay rate, T_2' , could be estimated by:

$$e^{-\frac{t}{T_2'}} \sim \int e^{i(\Omega - \omega(\vec{r}))t}$$

$$\varphi(r, t) = (\Omega - \omega(r)) \cdot t + \phi_0$$

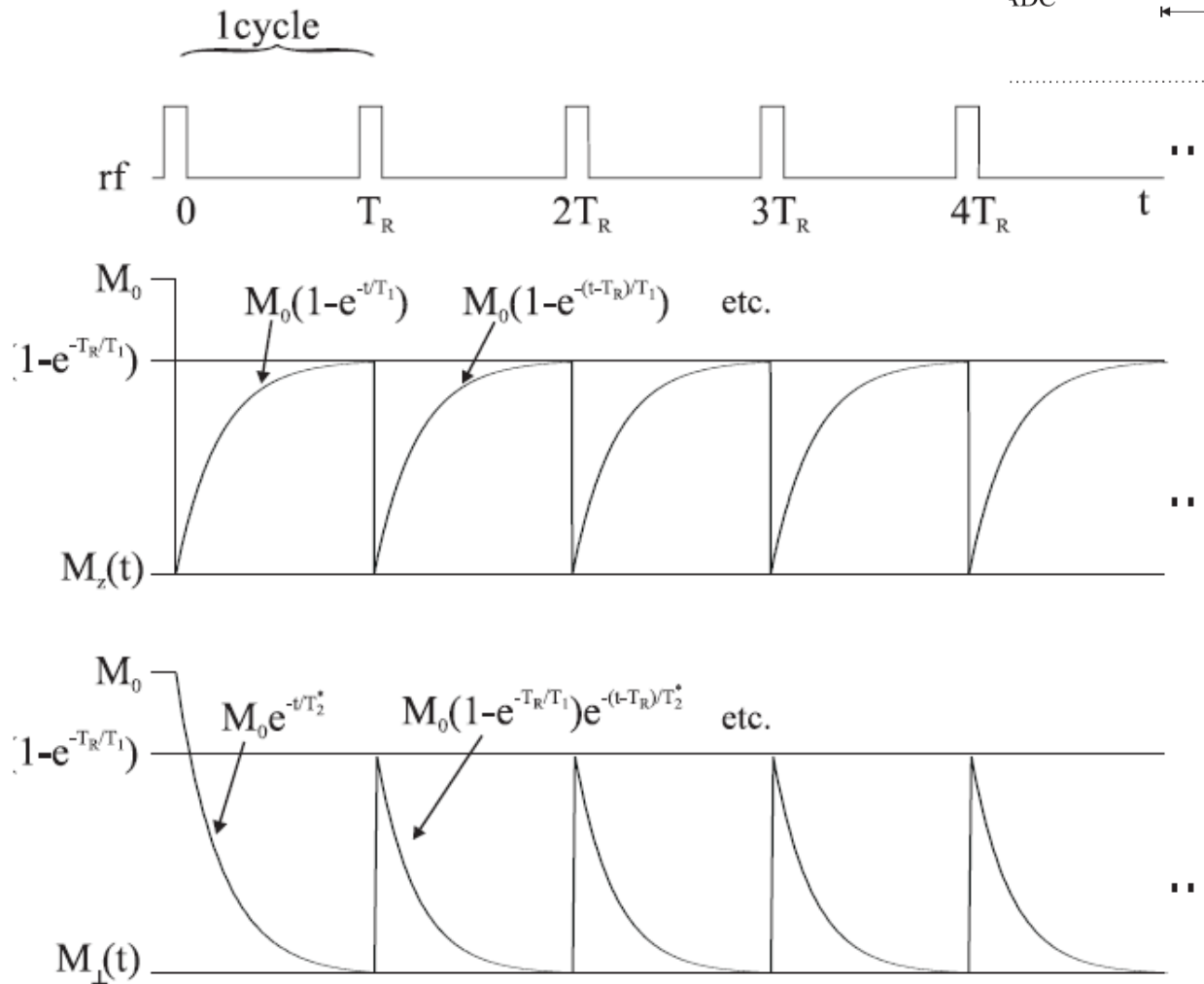
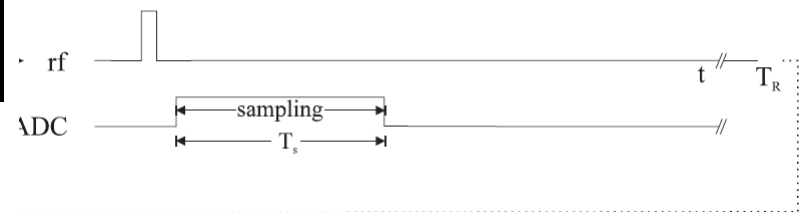
$$\varphi(r, t) = \gamma(B_0 - B(r)) \cdot t + \phi_0$$

$$\varphi(r, t) = \gamma(B_0 - (B_0 + \Delta B(r))) \cdot t + \phi_0$$

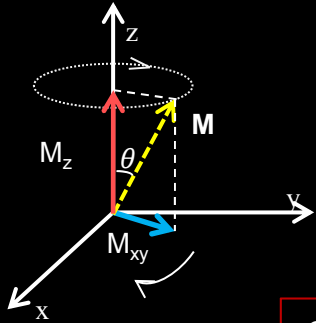
$$\varphi(r, t) = -\gamma \cdot \Delta B(r) \cdot t + \phi_0$$

$$e^{-\frac{t}{T_2'}} \sim \int e^{i\varphi(r, t)}$$

Multi-pulse experiments



Magnetization equations



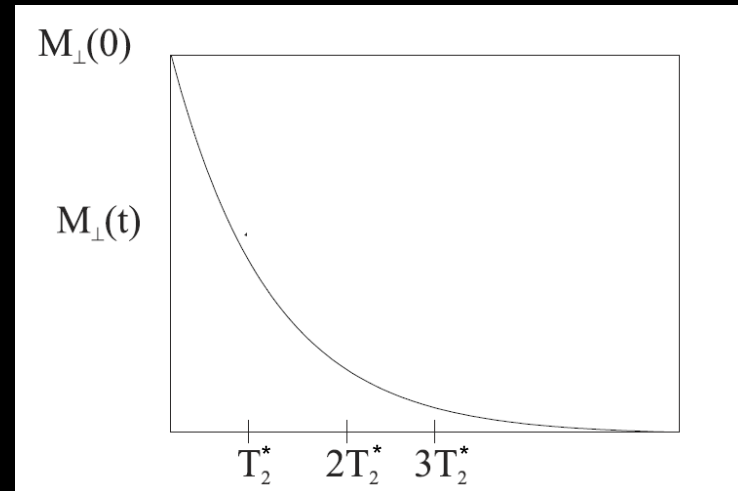
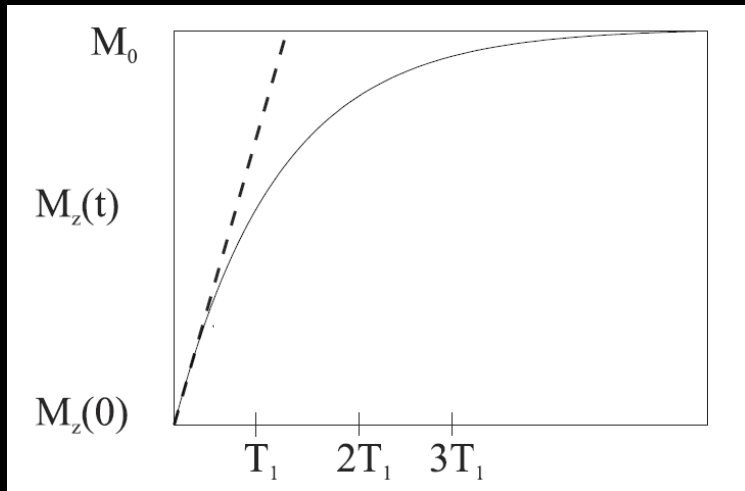
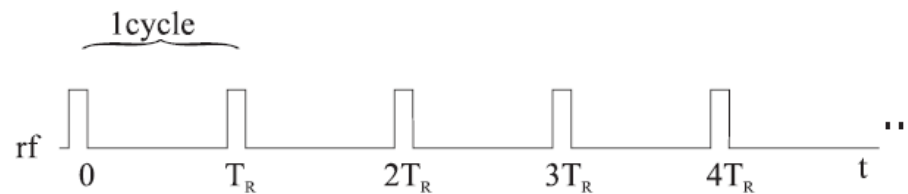
$$\theta = 90^\circ$$

$$M_z(t) = M_z(0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot (1 - e^{-\frac{t}{T_1}})$$

$$M_z(0) = M_0 \cdot \cos(\theta)$$

$$M_{xy}(t) = M_{xy}(0) \cdot e^{-\frac{t}{T_2^*}}$$

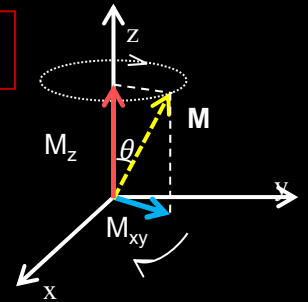
$$M_{xy}(0) = M_0 \cdot \sin(\theta)$$



$$TR \gg T_2^*$$

FID sampling and repeated scans

$$\theta = 90^\circ$$



With a 90° excitation:

$$TR \gg T_2^*$$

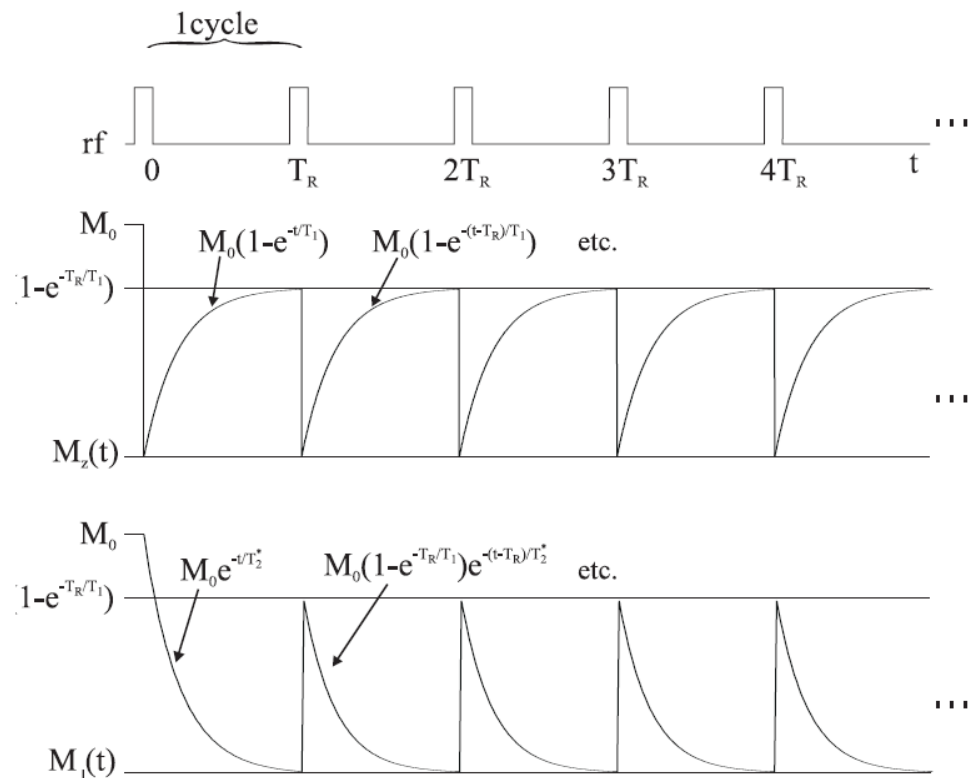
$$\begin{cases} M_z(0^+) = 0 \\ M_\perp(0^+) = M_0 \end{cases}$$

$$\begin{cases} M_z(TR^-) = M_0(1 - e^{-TR/T_1}) \\ M_\perp(TR^-) = M_0 e^{-TR/T_2^*} \end{cases}$$

...

$$\begin{cases} M_z(nTR^-) = M_0(1 - e^{-TR/T_1}) \\ M_\perp(nTR^-) = M_0(1 - e^{-TR/T_1})e^{-TR/T_2^*} \end{cases}$$

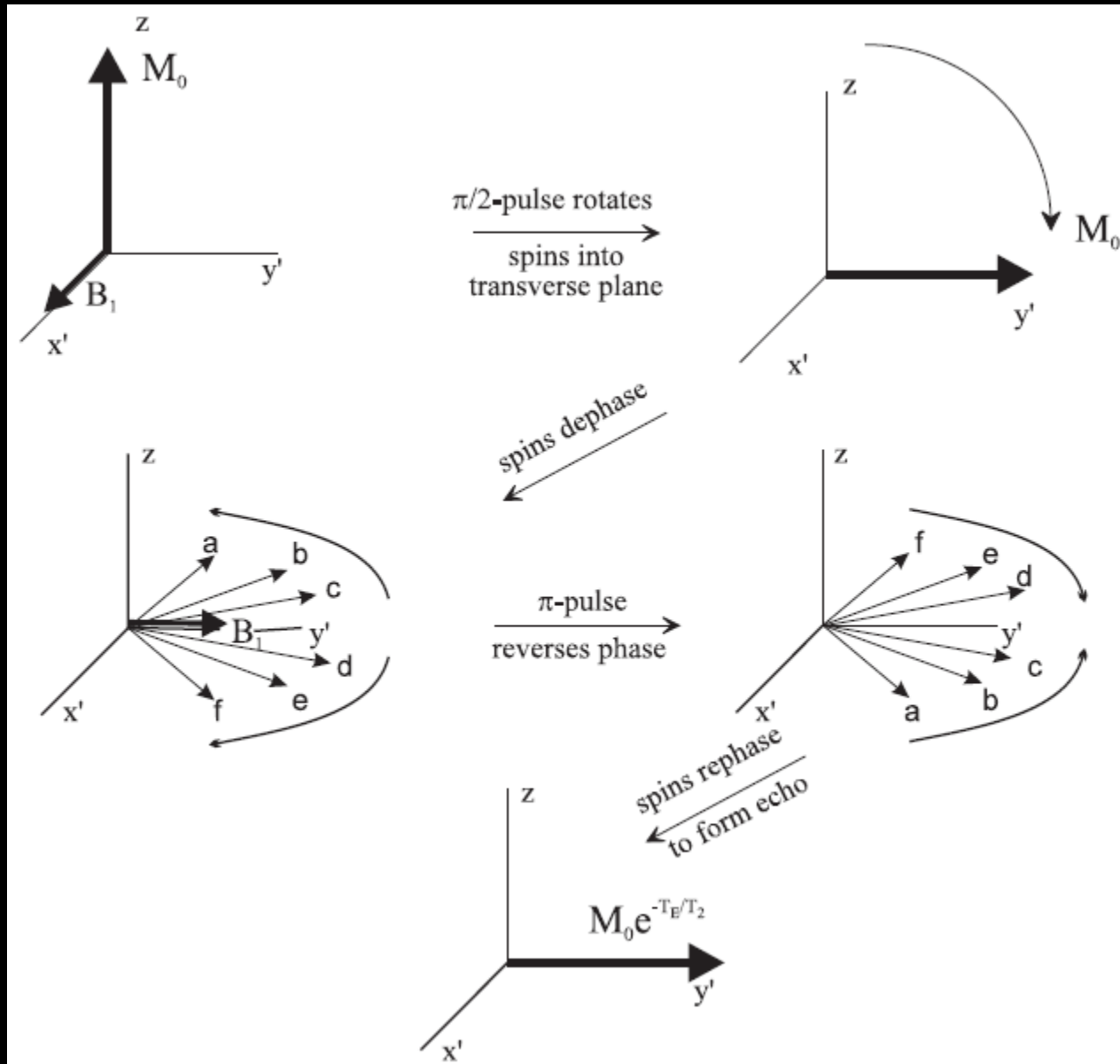
Note that both T_1 and T_2^* affect the signal's amplitude



Spin echo (rf echo)

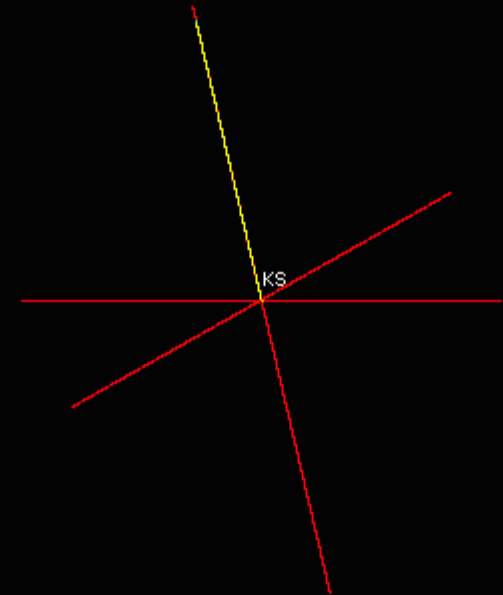
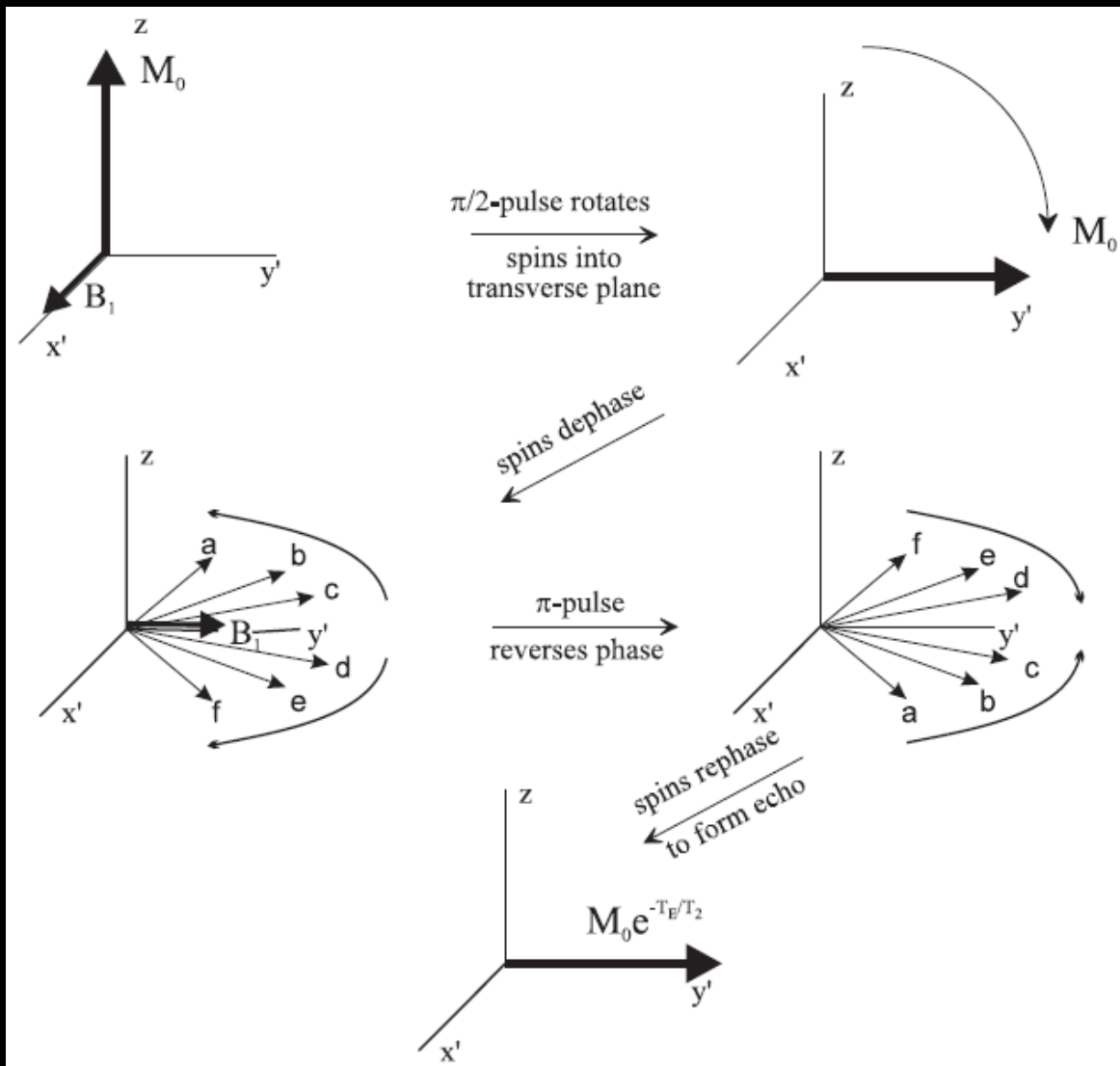
$\pi/2$ rf pulse
about the x'
axis

π refocusing rf
pulse about the
 y' axis

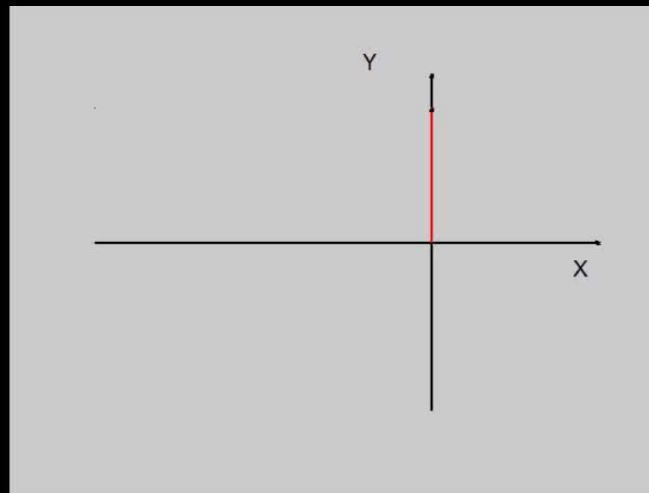
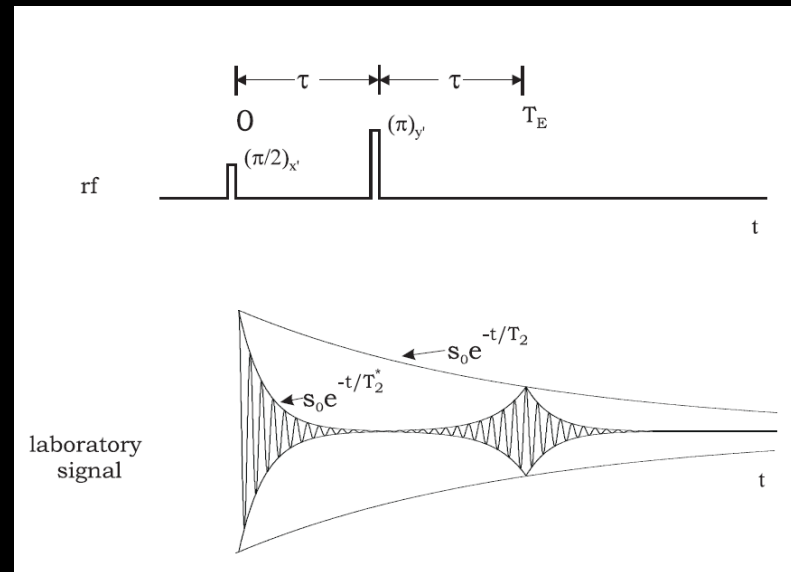
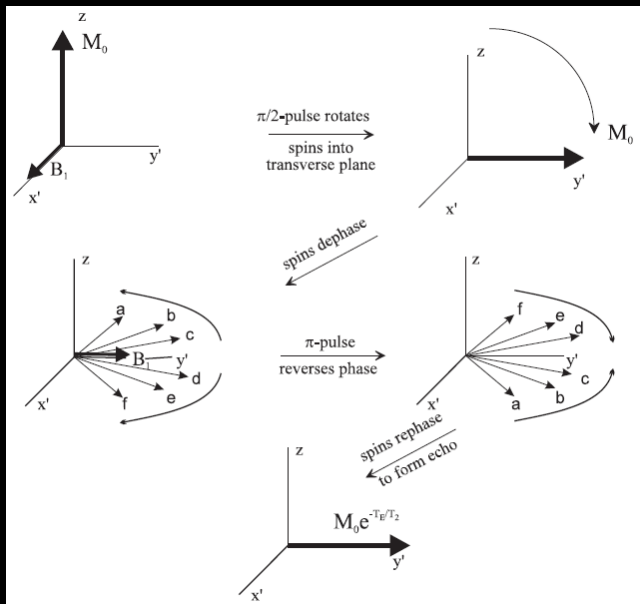


Echo occurs
along the y'
axis

Spin echo (rf echo)



Spin echo (rf echo)



Spin echo (rf echo)

How SE works

$$1. \phi(\vec{r}, t) = -\gamma \Delta B(\vec{r}) t, 0 < t < \tau$$

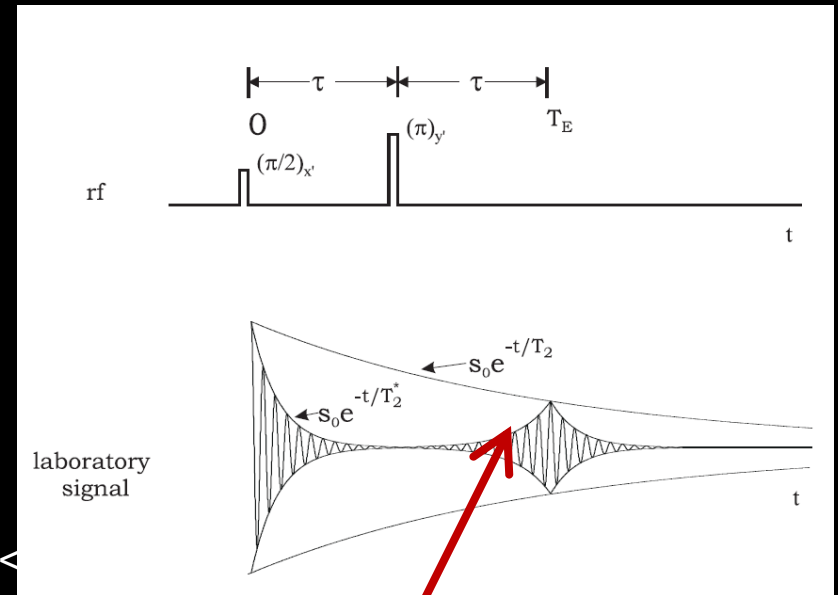
Refocusing π pulse after time τ ...

$$2. \phi(\vec{r}, \tau^+) = -\phi(\vec{r}, \tau^-) = \gamma \Delta B(\vec{r}) \tau, t = \tau$$

$$3. \phi(\vec{r}, t) = -\gamma \Delta B(\vec{r})(t - \tau) + \gamma \Delta B(\vec{r}) \tau, \tau < t < 2\tau$$

$$4. \phi(\vec{r}, 2\tau) = 0, t = 2\tau \equiv TE$$

$$5. \phi(\vec{r}, t) = -\gamma \Delta B(\vec{r})(t - 2\tau), t > 2\tau$$

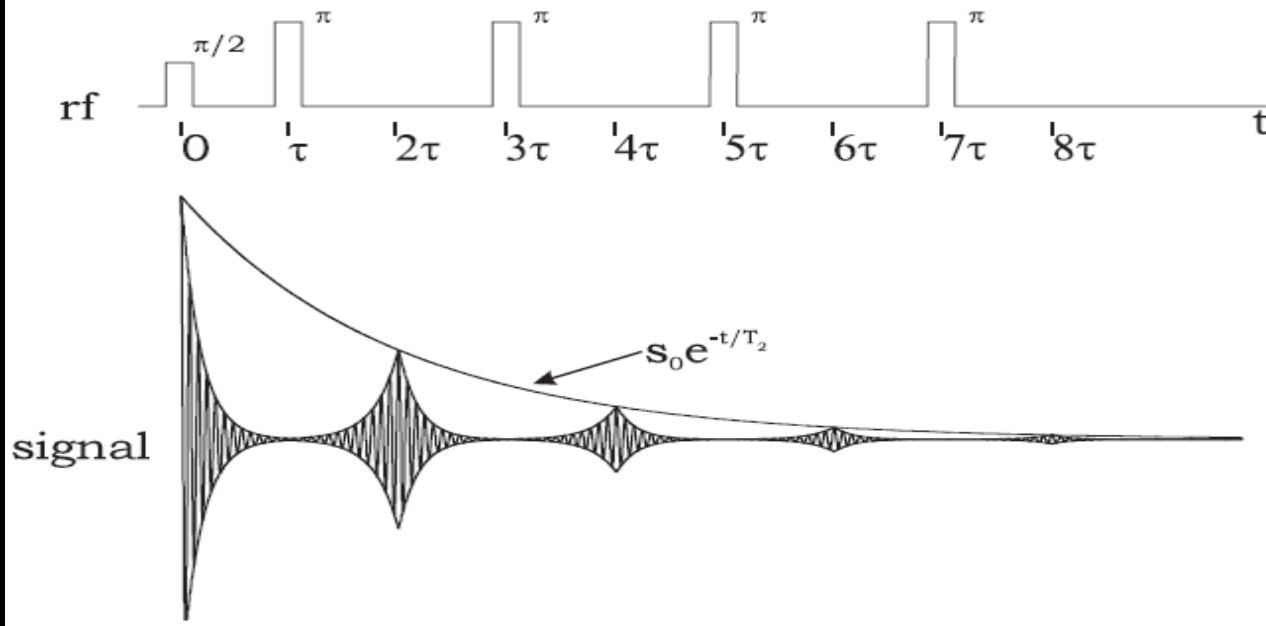
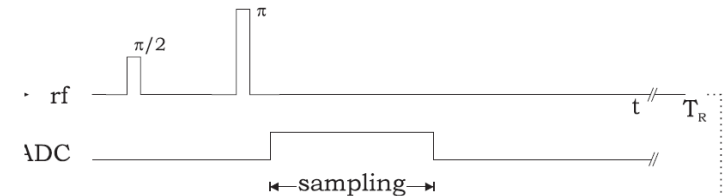


$$S(t) = S_0 \cdot e^{-t \left(\frac{1}{T_2} - \frac{1}{T_2^*} \right)}$$

T_2^* dephasing continues...

Multi-echo Spin Echo

$$TR \gg T_2^*$$



$$S(T E_1) = S_0 \cdot e^{-\frac{T E_1}{T_2}}$$

$$S(T E_2) = S_0 \cdot e^{-\frac{T E_2}{T_2}}$$

$$T_2 = \frac{T E_2 - T E_1}{\ln \left(\frac{S(T E_1)}{S(T E_2)} \right)}$$

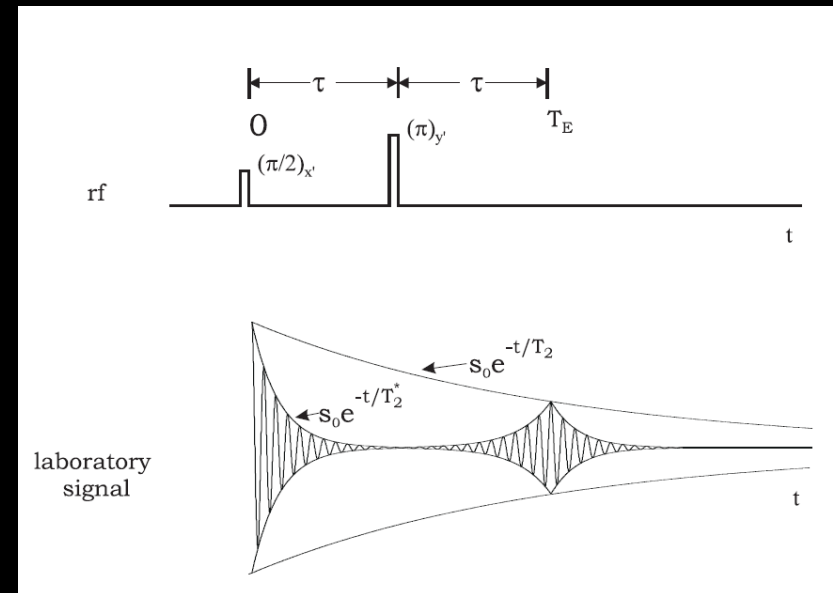
Note:

The phase of refocusing pulses greatly affects the signal of ME-SE. Consider the following rf pulse schemes:

- 1) $90^\circ(x) - 170^\circ(y) - 170^\circ(y) - 170^\circ(y) - 170^\circ(y) \dots$
- 2) $90^\circ(x) - 170^\circ(y) - 170^\circ(-y) - 170^\circ(y) - 170^\circ(-y) \dots$ (CPMG seq)

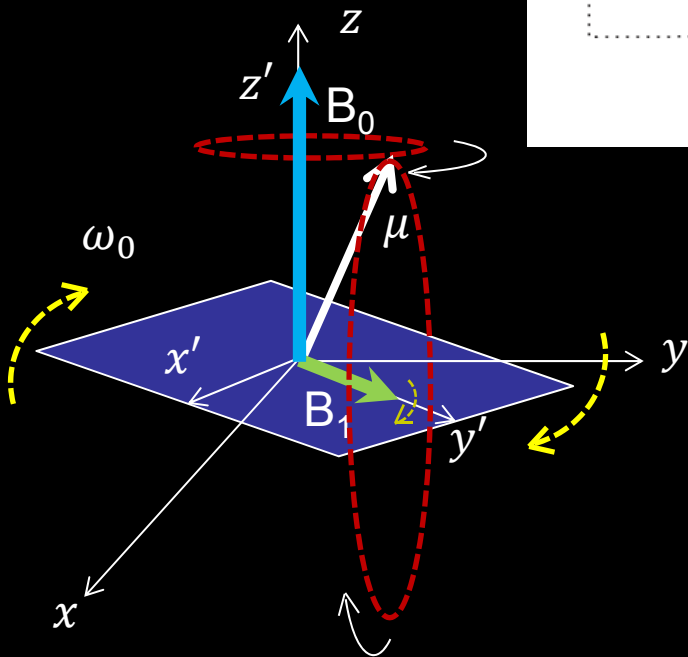
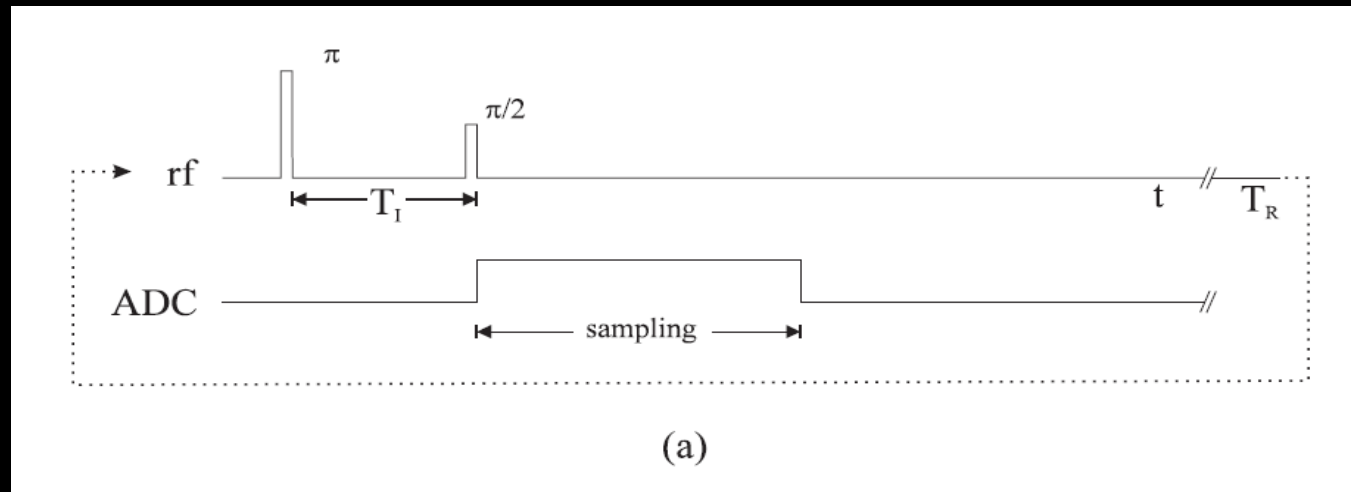
T2

- Maximal signal limited to T2 decay which is not recoverable
- T2' decay on both sides of the echo acts as low pass filter, blurring the image (Chap. 13)
- True T2 is difficult for precise quantification
 - Motion, partial volume effects, RF pulse, data acquisition, etc.
- Extra consideration for multiple spin echo acquisition
 - RF pulse phase
 - RF energy deposition
 - Multiple signal pathways ($TR < T_2^*$)
- Long scan time



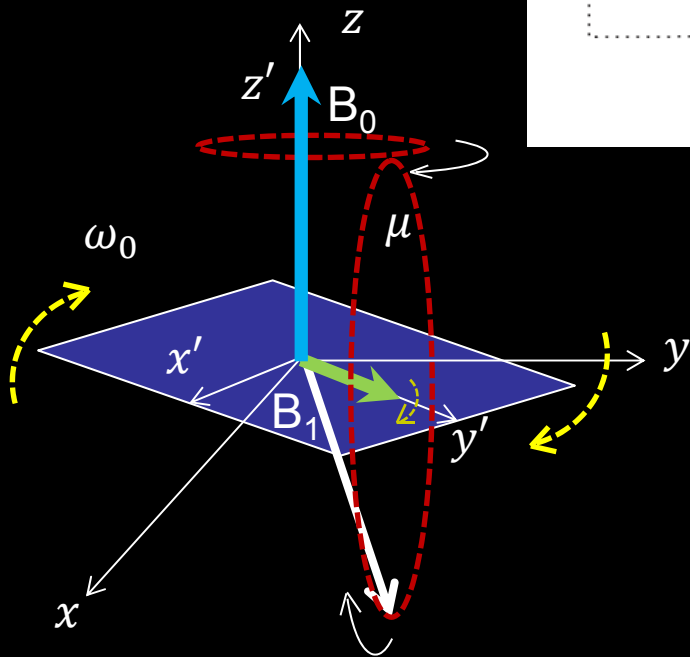
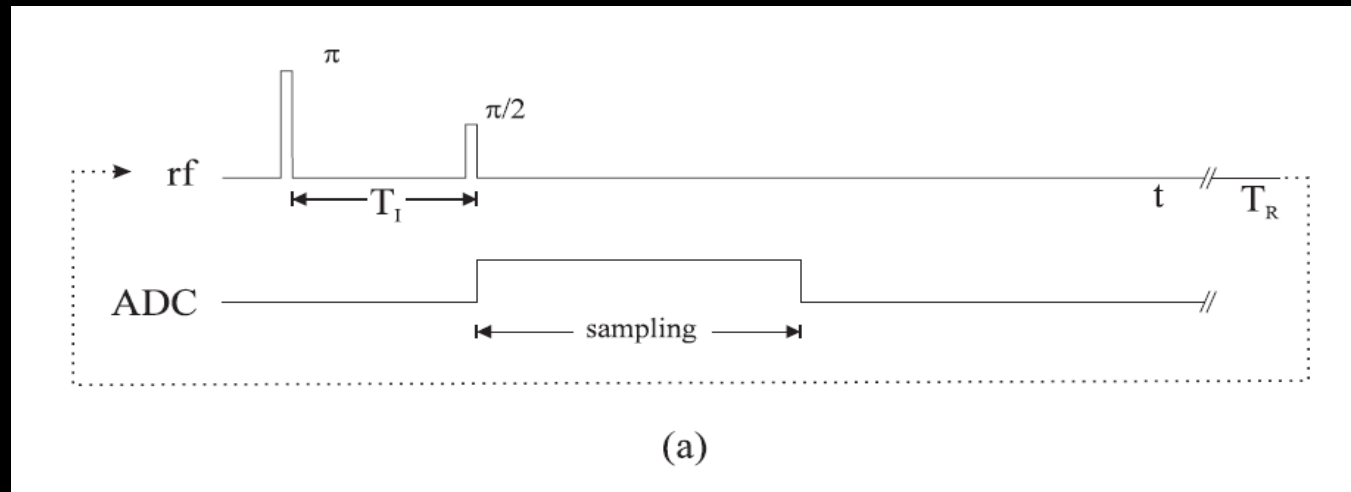
Inversion Recovery

$$M_z(t) = M_z(t = 0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot \left(1 - e^{-\frac{t}{T_1}}\right)$$



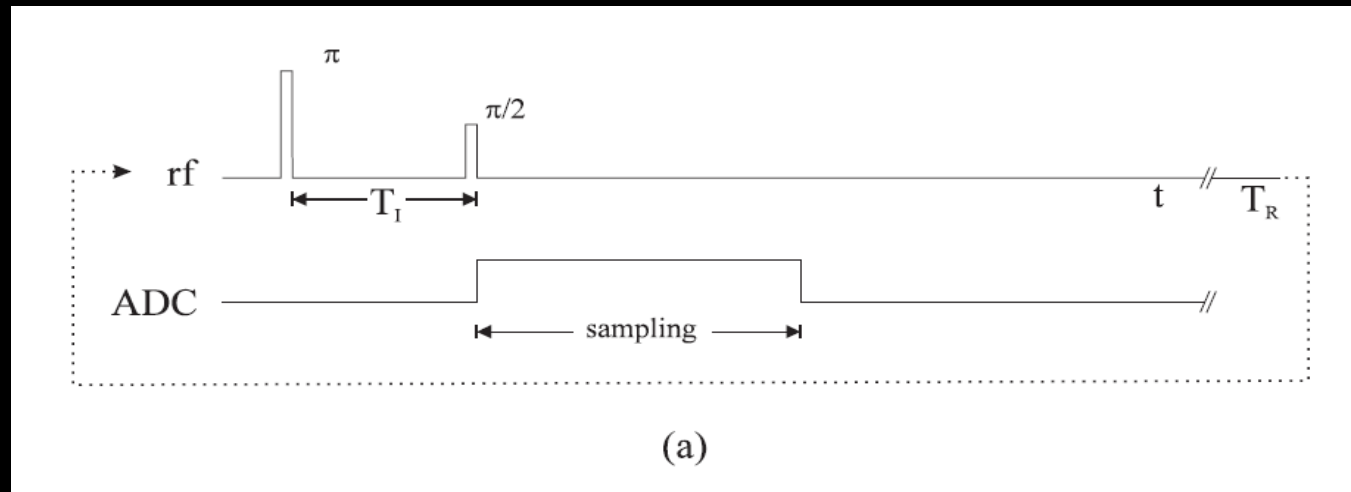
Inversion Recovery

$$M_z(t) = M_z(t = 0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot \left(1 - e^{-\frac{t}{T_1}}\right)$$



Inversion Recovery

$$M_z(t) = M_z(t = 0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot \left(1 - e^{-\frac{t}{T_1}}\right)$$



$$M_z(0^+) = -M_0$$

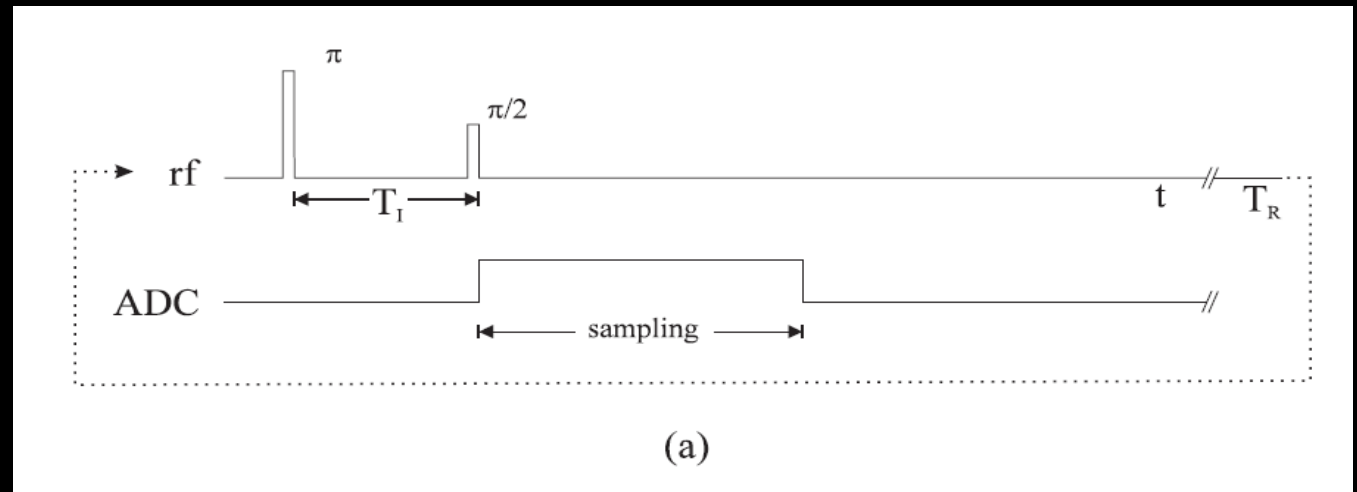
$$M_z(t) = -M_0 e^{-t/T_1} + M_0(1 - e^{-t/T_1}) = M_0(1 - 2e^{-t/T_1})$$

$$0 < t < T_I$$

$$M_{\perp}(t) = \left| M_0(1 - 2e^{-T_I/T_1}) \right| e^{-(t-T_I)/T_2^*}, \quad t > T_I$$

Inversion Recovery

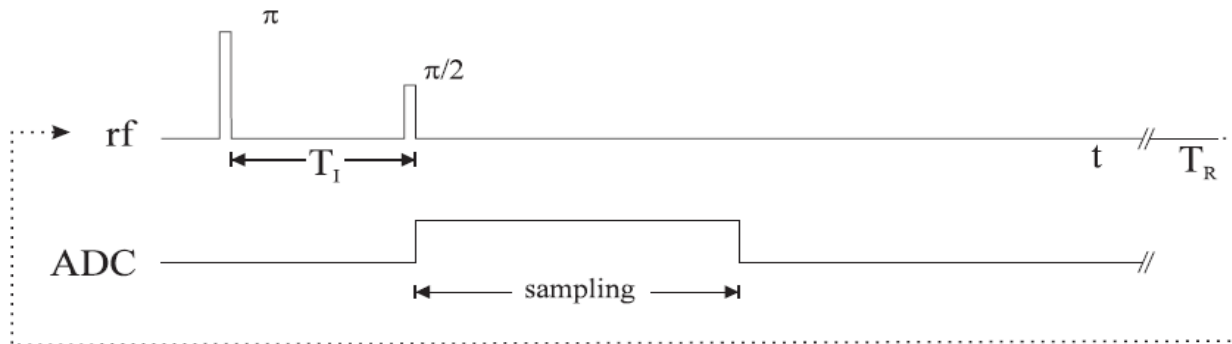
$$M_z(t) = M_z(t = 0) \cdot e^{-\frac{t}{T_1}} + M_0 \cdot \left(1 - e^{-\frac{t}{T_1}}\right)$$



$$M_{\perp}(t) = \left| M_0(1 - 2e^{-T_I/T_1}) \right| e^{-(t-T_I)/T_2^*}, \quad t > T_I$$

$$T_{I,null} = T_1 \ln 2$$

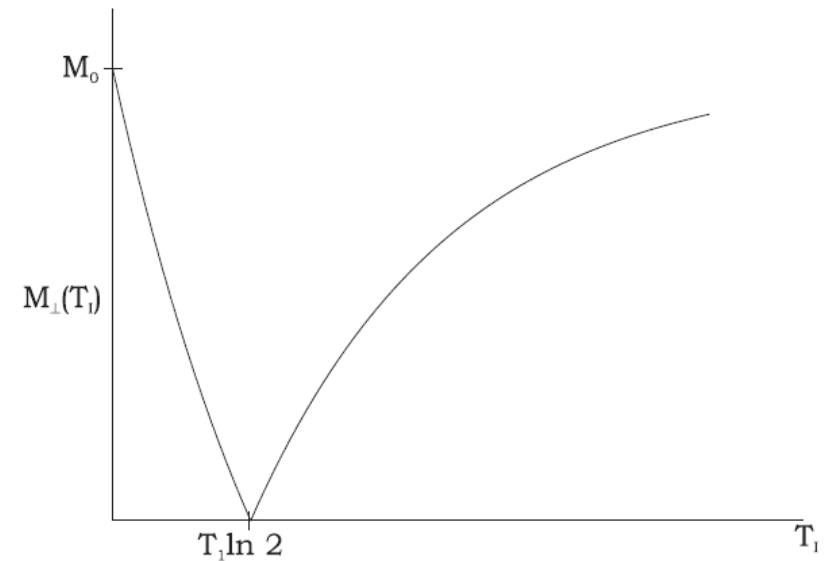
Inversion Recovery



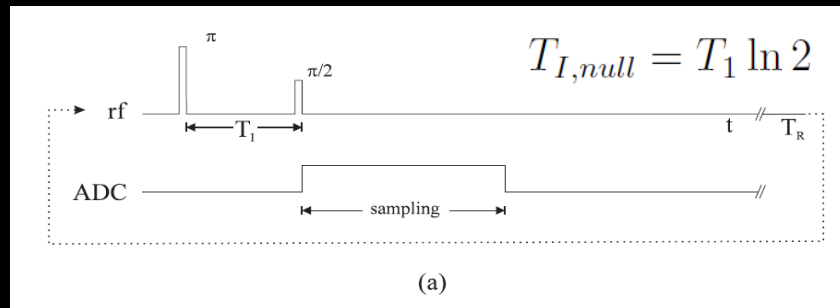
(a)

$$T_{I,null} = T_1 \ln 2$$

By sampling the signal at varying T_I s (inversion time), T_1 of a tissue could be quantified

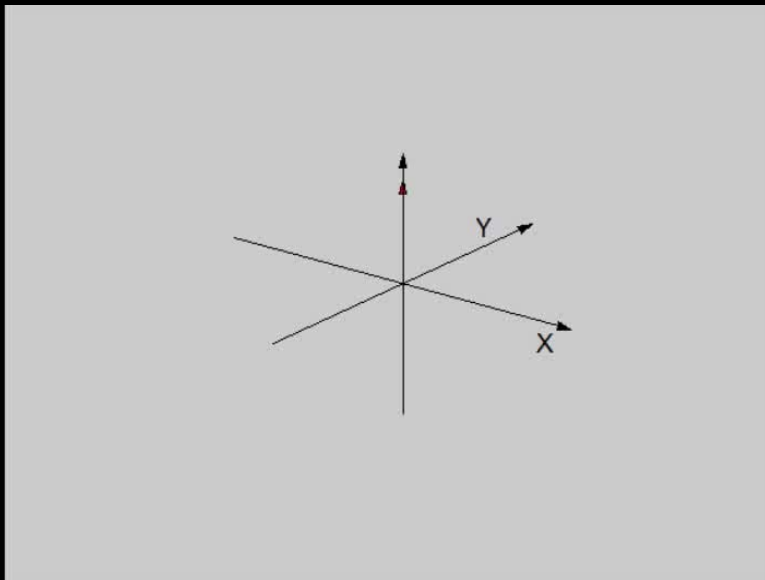


Inversion Recovery

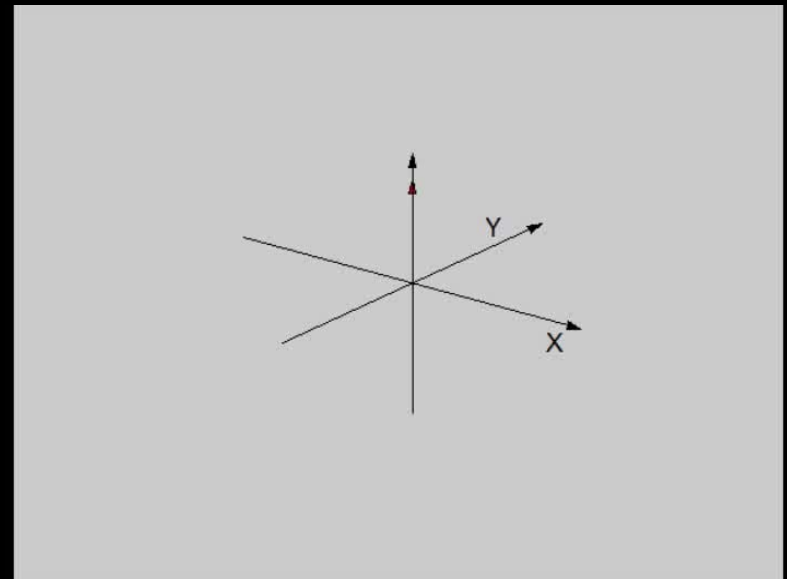


Can also be used to null the signal from a tissue by appropriately timing the $\pi/2$ pulse if the T_1 of the tissue is known

$$T_1 = 300/1000 \text{ ms}$$

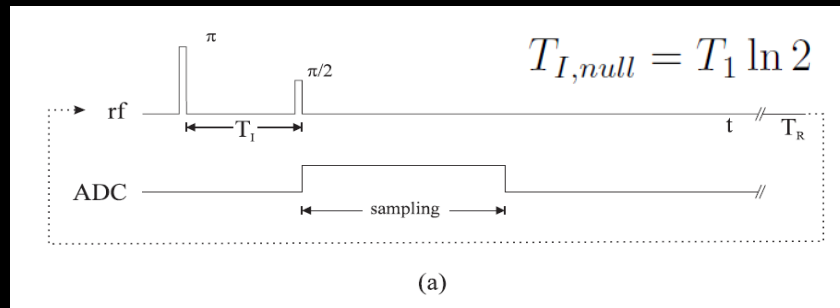


$T_I = 100 \text{ ms}$



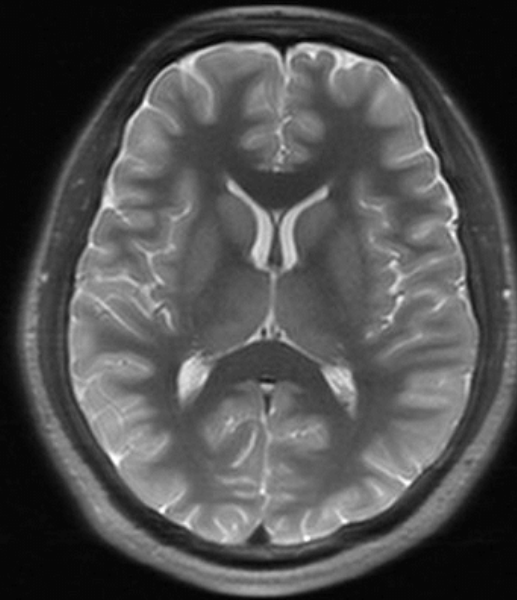
$T_I = 208 \text{ ms}$

Inversion Recovery



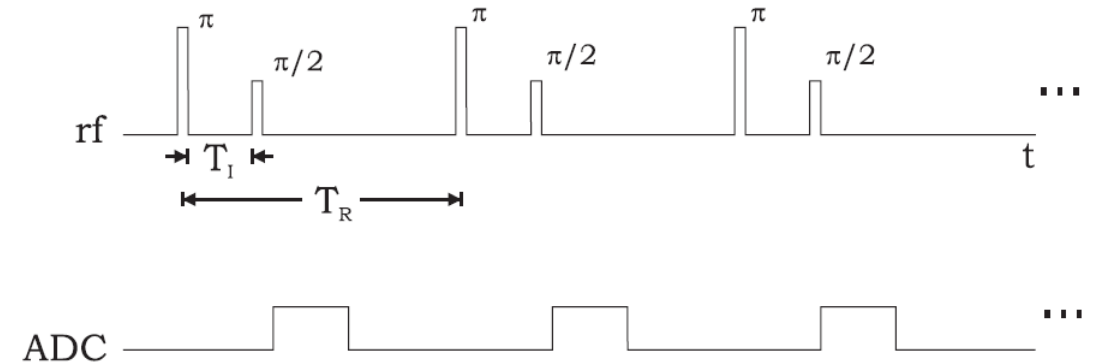
Can also be used to null the signal from a tissue by appropriately timing the $\pi/2$ pulse if the T_1 of the tissue is known

$$T_1 = 300/1000 \text{ ms}$$



Images acquired with different inversion times
(TIs from 100 to 1500 msec @1.5T)

Repeated IR scans



$$M_z(0^+) = -M_z(0^-) = -M_0$$

$$M_{\perp}(0^+) = 0$$

$$M_z(t) = -M_z(0^-)e^{-t/T_1} + M_0(1 - e^{-t/T_1}) = M_0(1 - 2e^{-t/T_1})$$

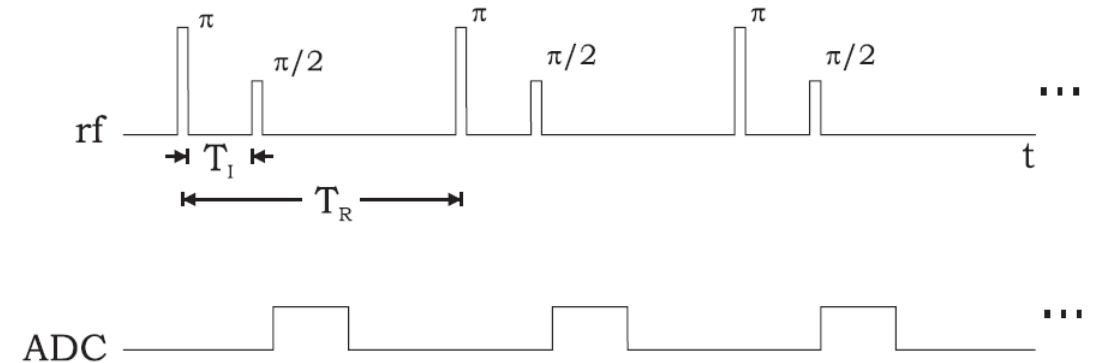
$$M_{\perp}(t) = 0$$

$$0 < t < T_I$$

$$M_z(T_I^+) = 0$$

$$M_{\perp}(T_I^+) = \left| -M_z(0^-)e^{-T_I/T_1} + M_0(1 - e^{-T_I/T_1}) \right| = |M_0(1 - 2e^{-T_I/T_1})|$$

Repeated IR scans



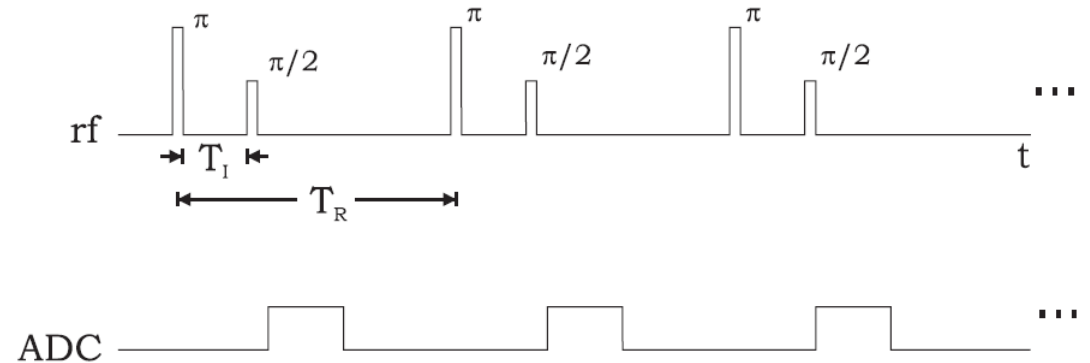
$$M_z(t) = M_0 \left(1 - e^{-(t-T_I)/T_1} \right)$$

$$\begin{aligned} M_{\perp}(t) &= \left| -M_z(0^-)e^{-T_I/T_1} + M_0(1 - e^{-T_I/T_1}) \right| e^{-(t-T_I)/T_2^*} \\ &= \left| M_0(1 - 2e^{-T_I/T_1}) \right| e^{-(t-T_I)/T_2^*} \end{aligned}$$

$$T_I < t < T_R$$

$$M_z(T_R^-) = M_0 \left(1 - e^{-(T_R-T_I)/T_1} \right)$$

Repeated IR scans



$$\begin{aligned}
 M_{\perp}(t_n) &= \left| -M_0(1 - e^{-(T_R - T_I)/T_1})e^{-T_I/T_1} + M_0(1 - e^{-T_I/T_1}) \right| e^{-(t_n - T_I)/T_2^*} \\
 &= M_0 \left| 1 + e^{-T_R/T_1} - 2e^{-T_I/T_1} \right| e^{-(t_n - T_I)/T_2^*} \\
 &\quad T_I < t_n < T_R
 \end{aligned}$$

$$T_{I_{\text{null}}} = T_1 \ln \left(\frac{2}{1 + e^{-T_R/T_1}} \right)$$

Homework

- Prob. 8.1-8.5

Next Class

Chapter 9.1-9.4